# Modeling and simulation of mechano-chemical pattern formation processes

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Thomas Richter
University of Magdeburg
Institute for Analysis and Numerics

with Felix Brinkmann, University of Heidelberg

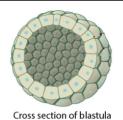
Moritz Mercker, University of Heidelberg and Anna Marciniak-Czochra, University of Heidelberg

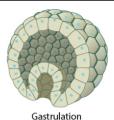
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# **Overview**

- Motivation
- Modeling
- Numerics & Results







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# Theories explaining pattern formation processes

- 1. A sequence of successive chemical patterns form. This would rule out spontaneous self-organized processes, as they are observed in dissociated and re-aggregated cells.
- 2. Chemical patterns can form spontaneously by an interplay of mutual interaction of diffusing morphogens by the *Turing mechanism*. While the *Turing mechanism* creates many relevant patterns, experiments usually do not find morphogens with requires diffusion and reaction rates.

Turing: The chemical basis of morphogenesis, Phil. Trans. R. Soc. London, 1953

Meinhardt & Gierer: Pattern formation by local self-activation and lateral inhibition, Bioessays, 2000

• Both theories say, that mechanical patterns are *blind end results* of chemical pre-patterns. Recent studies however show, that mechanical patterns play an *active role*.

Brouzes & Farge: Interplay of mechanical deformation and patterned gene expression in developing embryos, Curr. Opin. Genet. Dev., 2004

### Mechanics

$$-\operatorname{div}\left(\mathbf{F}\boldsymbol{\Sigma}\right) = 0 \text{ in V},$$

assuming a St. Venant Kirchhoff material

$$\Sigma = 2\mu \mathbf{E} + \lambda \operatorname{tr}(\mathbf{E})I, \quad \mathbf{E} = \frac{1}{2}(\mathbf{F}^T \mathbf{F} - I), \quad \mathbf{F} = I + \nabla \mathbf{u}$$

With

$$\mathbf{u} = 0 \text{ on } \Gamma_D, \quad \mathbf{F} \mathbf{\Sigma} \mathbf{n} = g \text{ on } \Gamma_N$$

We assume, that growth is very slow compared to elastic dynamics such that the mechanical system is always in a stationary limit

# (Bio-)Chemistry

System of reaction diffusion equations (in Lagrangian coordinates)

$$J\partial_t c_i - \operatorname{div}\left(J\mathbf{F}^{-1}D\mathbf{F}^{-T}\nabla c_i\right) - JR_i(c_1,\ldots,c_n) = 0 \text{ in } V \text{ for } i=1,\ldots,n$$

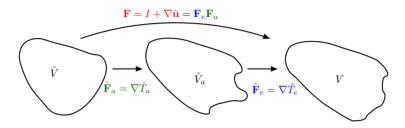
with initial and boundary conditions

$$c_i = c_i^0$$
 for  $t = 0$  and  $J\mathbf{F}^{-1}D\mathbf{F}^{-T}\nabla c_i\mathbf{n} = 0$  on  $\Gamma$ 

• Intermediate configuration

$$\hat{V} \xrightarrow{\hat{T}_a} \hat{V}_a \xrightarrow{\hat{T}_e} V$$

• Active deformation  $\hat{T}_a$  and elastic deformation  $\hat{T}_e$ 



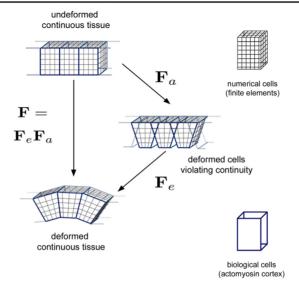
# Elasticity takes place between $V_a$ and V

$$\Sigma = \Sigma(\mathbf{F}_e) = \Sigma(\mathbf{F}\mathbf{F}_a^{-1})$$

For the St. Venant Kirchhoff material

$$\Sigma = J_a \mathbf{F}_a^{-1} \Sigma_e \mathbf{F}_a^{-T}, \quad \Sigma_e = 2\mu \mathbf{E}_e + \lambda \operatorname{tr}(\mathbf{E}_e) I, \quad \mathbf{E}_a = \frac{1}{2} (\mathbf{F}_e^T \mathbf{F}_e - I) = \frac{1}{2} (\mathbf{F}_a^{-T} \mathbf{F}^T \mathbf{F} \mathbf{F}_a^{-1} - I).$$

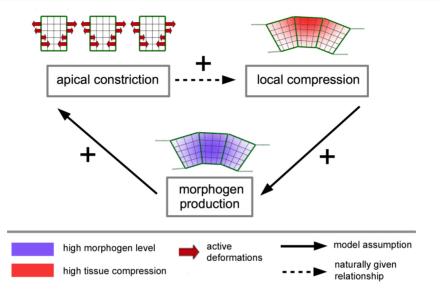
Rodriguez, Hoger & McCulloch: Stress-depedent finite growth in soft elastic tissues, J. BioMech. 1994 Ambrosi & Mollica: On the mechanics of a growing tumor, IJ Eng. Science 2002



 $\bullet$  Active deformation (here apical constriction) depends on one chemical concentration c

$$\hat{\mathbf{F}}_a(x,y,z,\mathbf{c})\Big|_M = \begin{pmatrix} 1 + \kappa \mathbf{c} \hat{z} & 0 & \kappa \mathbf{c} \hat{x} \\ 0 & 1 + \kappa \mathbf{c} \hat{z} & \kappa \mathbf{c} \hat{y} \\ 0 & 0 & 1 \end{pmatrix}, \quad \begin{pmatrix} \hat{x} \\ \hat{y} \\ \hat{z} \end{pmatrix} = \begin{pmatrix} x - x_M \\ y - y_M \\ z - z_M \end{pmatrix} \text{ rel. to midpoint of cell } M$$

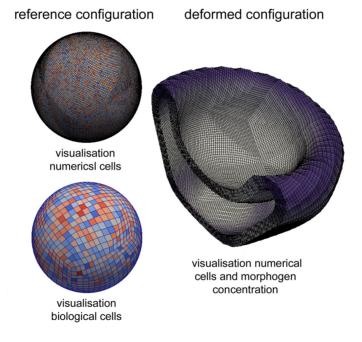
• (Simplified, as we first have to rotate every biological cell to a reference orientation)



- High morphogen level causes apical constriction  $\mathbf{F}_a = \mathbf{F}_a(c)$
- Apical constriction causes elastic feedback with local compression  $\Sigma_e = \Sigma(\mathbf{F}\mathbf{F}_a^{-1})$
- Local compression triggers morphogen production (Michaelis-Menten kinetics)

$$R(c, \mathbf{F}) = \kappa_1 \frac{\max\{\det \mathbf{F}, 0\}}{\kappa_3 + \max\{\det \mathbf{F}, 0\}} - \kappa_2 c, \quad \kappa_1, \kappa_2, \kappa_3 > 0$$

- We consider a layer of biological cells. The (adaptive) finite element discretization is much finer
- Overall very large active and elastic deformation appears



### Monolithic Model

$$U = \{\mathbf{u}, \mathbf{c}\} \in \mathcal{X} : A(U)(\Phi) = 0 \quad \forall \Phi \in \mathcal{X}$$

The variational formulation is given by

$$A(U)(\Phi) = (\mathbf{F} J_a \mathbf{F}_a^{-1} \mathbf{\Sigma}_e \mathbf{F}_a^{-T}, \nabla \phi) + (J \partial_t c, \psi) + (J \mathbf{F}^{-1} D \mathbf{F}^{-T} \nabla c, \nabla \psi) - (J R(c, \mathbf{F}), \psi)$$

with

• Growth model

$$\hat{\mathbf{F}}_a \Big|_M = egin{pmatrix} 1 + \kappa c \hat{z} & 0 & \kappa c \hat{x} \\ 0 & 1 + \kappa c \hat{z} & \kappa c \hat{y} \\ 0 & 0 & 1 \end{pmatrix}$$

• Reaction feedback

$$R(c, \mathbf{F}) = \kappa_1 \frac{\max\{\det \mathbf{F}, 0\}}{\kappa_3 + \max\{\det \mathbf{F}, 0\}} - \kappa_2 c$$

• Stress model with growth-splitting

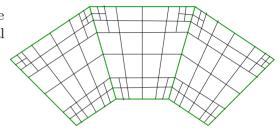
$$\Sigma_e = 2\mu \mathbf{E}_e + \lambda \operatorname{tr}(\mathbf{E}_e), \quad \mathbf{E}_e = \frac{1}{2} (\mathbf{F}_a^{-T} \mathbf{F}^T \mathbf{F} \mathbf{F}_a^{-1} - I),$$
$$\mathbf{F} = I + \nabla \mathbf{u}$$

• Quadratic finite elements (3 deformation variables + 1 concentration)

$$X_h \subset \mathcal{X}, \quad X_h := \{ \phi \in C(\bar{\Omega})^{3+1}, \ \phi \big|_K \in Q^2(K)^4 \ \forall K \in \Omega_h \}$$

- Adaptive Meshes to efficiently resolve biological cells (there are jumps in the active growth model  $\mathbf{F}_a$  at the biological cell boundaries)
- Monolithic coupled approach

Find 
$$U_h = (\mathbf{u}_h, c_h) \in X_h$$
:  $A(U_h)(\Phi_h) = 0 \quad \forall \Phi_h \in X_h$ 



• Time stepping with the implicit Euler method. We found, that temporal accuracy is of lesser important (compared to spatial accuracy and stability problems)

### Nonlinear Solver

Linearization with Newton's method

$$A'(U_h^{(i)})(W_h^{(i)}, \Phi_h) = F(\Phi_h) - A(U_h^{(i)})(\Phi_h) \quad \forall \Phi_h \in X_h, \quad U_h^{(i+1)} = U_h^{(i)} + \omega W_h^{(i)}$$

Analytic computation of the monolithic Jacobian

• Large and ill-structure linear system of equations (couplings to elasticity  $\mathbf{A}$  to growth  $\mathbf{A}_G$  chemistry transport  $\mathbf{M}$ , diffusion  $\mathbf{A}_d$ , reaction  $\mathbf{A}_R$  and mapping to Lagrangian coordinates  $\mathbf{A}_E$ 

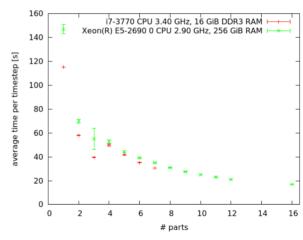
$$\begin{pmatrix} \mathbf{A} & \mathbf{A}_G \\ \mathbf{A}_R + \mathbf{A}_E & k^{-1}M + \mathbf{A}_d \end{pmatrix} \begin{pmatrix} \delta \mathbf{u} \\ \delta c \end{pmatrix} = \begin{pmatrix} \mathbf{b}_{\mathbf{u}} \\ \mathbf{b}_c \end{pmatrix}$$

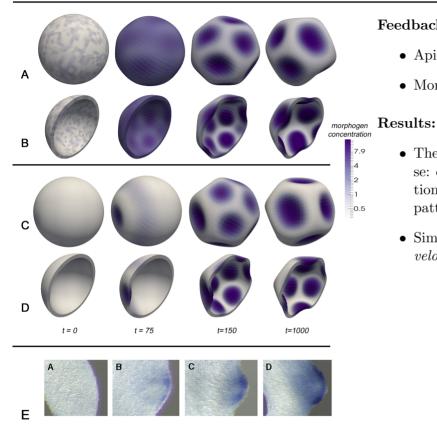
• Multigrid solver for the linear systems

$$Ax = b$$

• Parallelization of the multigrid solver by a domain decomposition smoother

- Highly complex simulations (nonlinearity and ill-structured linear systems)
- Fine meshes are required
- About 20 seconds per time-step
- Total simulation time in 3d about 10 days

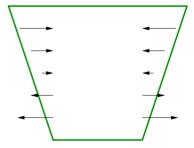


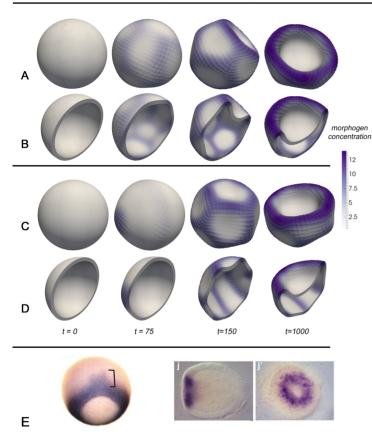


### Feedback Mechanism:

- Apical constriction
- Morphogen production by compression

- The process is stable in the following sense: different initial morphogen concentrations give the same stationary mechanical pattern
- Similar patterns are observed in *Hydra de*velopment



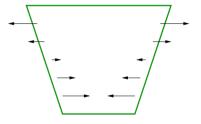


### Feedback Mechanism:

- Basal constriction
- Morphogen production by compression

### Results:

- Again, stable process
- Similar results are found in Nematostella and Xenopus gastrulation.



# **Further Steps**

### • Numerical Simulation

We identify possible feedback-loops and mechanisms

- What is the trigger for morphogen production? Cell-size or shape  $\mathbf{F}$ , elastic stress  $\Sigma_e$ , strain  $\mathbf{E}_e$  or  $\mathbf{E}$ ?
- How does the biological cell react?
   Compression, apical or basal constriction, shear, ...

### • Biological verification

Currently, experimentalists run experiments that are based on our simulations:

- Can we trigger morphogen-production by a mechanical stimulus?
- Can we produce a mechanical reaction by a injecting morphogens?

### • Mathematical Analysis

Is the coupled mechano-chemical system of partial differential equations well-posed?

- Stability estimates for the long-term simulations. Control of the chemical concentration and elastic stresses
- Design of robust and efficient solvers

# **Summary**

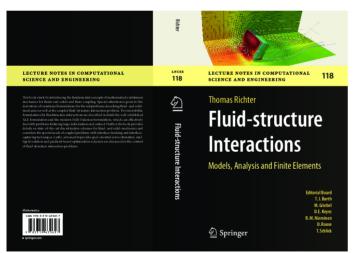
- Novel numerical model that is able to show spontaneous pattern formation processes based on an interplay of mechanics and bio-chemistry
- Robust high-performance framework for mechano-chemical coupled simulations

All computations done with Gascoigne 3D

# Upcoming thesis:

Felix Brinkmann: Mathematical models and numerical simulation of mechanochemical pattern formation in biological tissues, Dissertation, University of Heidelberg, 2017





- Y. Yang & T.R. & W. Jäger & M. Neuss-Radu: An ALE approach to mechano-chemical processes in fluid-structure interactions, Int. J. Numer. Meth. Fluids, 2017
- M. Mercker & F. Brinkmann & A. Marcinbia-Czochra & T.R.: Beyond Turing: Mechanochemical pattern formation in biological tissues, Biology Direct, 2016
- T.R.: Fluid-structure Interactions., Lecture Notes in Computational Science and Engineering 118, November 2017